NETWORK NEURO SCIENCE

an open access 🔓 journal



Citation: DuPre, E., & Spreng, R. N. (2017). Structural covariance networks across the life span, from 6 to 94 years of age. *Network Neuroscience*, *1*(3), 302–323. https://doi.org/10.1162/ netn_a_00016

DOI: https://doi.org/10.1162/netn_a_00016

Supporting Information: https://doi.org/10.1162/netn_a_00016

Competing Interests: The authors have declared that no competing interests exist.

Corresponding Author: R. Nathan Spreng nathan.spreng@gmail.com

Handling Editor: Olaf Sporns

Copyright: © 2017 Massachusetts Institute of Technology Published under a Creative Commons Attribution 4.0 International (CC BY 4.0) license



RESEARCH

Structural covariance networks across the life span, from 6 to 94 years of age

Elizabeth DuPre¹ and R. Nathan Spreng¹

¹Laboratory of Brain and Cognition, Human Neuroscience Institute, Department of Human Development, Cornell University, Ithaca, NY, USA

Keywords: Network, Structural covariance, Gray matter, Development, Aging, MRI

ABSTRACT

Structural covariance examines covariation of gray matter morphology between brain regions and across individuals. Despite significant interest in the influence of age on structural covariance patterns, no study to date has provided a complete life span perspective-bridging childhood with early, middle, and late adulthood-on the development of structural covariance networks. Here, we investigate the life span trajectories of structural covariance in six canonical neurocognitive networks: default, dorsal attention, frontoparietal control, somatomotor, ventral attention, and visual. By combining data from five open-access data sources, we examine the structural covariance trajectories of these networks from 6 to 94 years of age in a sample of 1,580 participants. Using partial least squares, we show that structural covariance patterns across the life span exhibit two significant, age-dependent trends. The first trend is a stable pattern whose integrity declines over the life span. The second trend is an inverted-U that differentiates young adulthood from other age groups. Hub regions, including posterior cingulate cortex and anterior insula, appear particularly influential in the expression of this second age-dependent trend. Overall, our results suggest that structural covariance provides a reliable definition of neurocognitive networks across the life span and reveal both shared and network-specific trajectories.

AUTHOR SUMMARY

The importance of life span perspectives is increasingly apparent in understanding normative interactions of large-scale neurocognitive networks. Although recent work has made significant strides in understanding the functional and structural connectivity of these networks, there has been comparatively little attention to life span trajectories of structural covariance networks. In this study we examine patterns of structural covariance across the life span for six neurocognitive networks. Our results suggest that networks exhibit both network-specific stable patterns of structural covariance as well as shared age-dependent trends. Previously identified hub regions seem to show a strong influence on the expression of these age-related trajectories. These results provide initial evidence for a multimodal understanding of structural covariance in network structure-function interaction across the life course.

INTRODUCTION

The human cerebral cortex is hierarchically organized into complex brain networks that can be considered at multiple levels of analysis (Mesulam, 1998). One such level is structural covariance, or how interindividual differences in regional brain structure covary with other Structural covariance: Interindividual differences in regional brain structure covarying with other brain structures across the population.

Neurocognitive networks: Large-scale, distributed neural networks associated with cognition. brain structures across the population (Alexander-Bloch, Giedd, & Bullmore, 2013; Mechelli, Friston, Frackowiak, & Price, 2005). Structural covariance networks reflect shared variation in gray matter morphology (Mechelli et al., 2005) and are assessed using measures such as cortical thickness and regional volume. These networks exhibit reproducible organization at both a population (Alexander-Bloch et al., 2013) and an individual (Tijms, Seris, Willshaw, & Lawrie, 2012) level and have been identified across species (Pagani, Bifone, & Gozzi, 2016), underscoring their role as an intrinsic feature of cortical organization. Despite this reliability, the source of gray matter shared covariance patterns is unclear and has been hypothesized to reflect both genetic and plastic influences, including maturational timing (Alexander-Bloch, Raznahan, Bullmore, & Geidd, 2013).

Age is a significant moderator of both anatomical (Collin & van den Heuverl, 2013; Hagmann et al., 2010) as well as functional (Chan, Park, Savalia, Petersen, & Wig, 2014; Dosenbach et al., 2010) connectivity. Some of the most extensive age effects occur in gray matter (Giorgio et al., 2010). Gray matter organization undergoes significant structural change with age, including synaptic proliferation, pruning, and eventual atrophy (Fjell et al., 2010; Low & Cheng, 2006). Normative gray matter changes do not occur simultaneously, however, and show variation across cortex (Krongold, Cooper, & Bray, 2017; Raz et al., 2005), yielding significant differences in age-related trajectories across structural covariance networks. There has therefore been substantial interest in the impacts of age on structural covariance networks, and how these age-related trajectories may differ across neurocognitive networks.

Investigations of structural covariance trajectories have largely focused on specific developmental periods, including childhood and adolescence (Zielinski, Gennatas, Zhou, & Seeley, 2010) or aging (Montembeault et al., 2012). These studies have suggested the emergence of increasing long-range structural covariance across early development (Zielinski et al., 2010) and increased local covariance with advancing age (Montembeault et al., 2012). Importantly, examining structural covariance networks in isolated developmental periods may limit our understanding of the normative life cycle of each of these networks (Zuo et al., 2017). Initial work examining trajectories over multiple developmental periods has found significant internetwork variation (Hafkemeijer et al., 2014).

There has also been increasing interest in examining structural covariance networks from a life span perspective. However, to date existing life span structural covariance studies (i.e., those spanning a minimum of 35 years of development; Zuo et al., 2017) have only included subjects with a minimum age of 18 years and considered differences between young-, middle-, or older-adult groups (Li et al., 2013; Wu et al., 2012). Results from these studies have largely been in agreement with those of individual developmental periods, with distributed structural covariance shifting to more local topology in older adulthood, though the timing of this transition is unclear and has differed between middle- (Wu et al., 2012) and younger- (Li et al., 2013) adulthood. Studies have also shown differences in structural covariance trajectories by network, with primary sensory and motor networks showing few to no age-related changes across adulthood, while neurocognitive and semantic networks show a general shift from distributed to local covariance (Li et al., 2013).

Despite this significant progress in understanding structural covariance during development and aging, the authors are unaware of any studies that have examined the development of large-scale structural covariance networks across the entire life span, including childhood and adolescence to old age. The changes seen in the developmental trajectory of large-scale functional networks (Zuo et al., 2017) suggest that a life span study of structural covariance

networks may provide an important complement, yielding insights into cortical organization at the level of gray matter morphology. Indeed, previous work by Zielinski and colleagues (2010) supports the reflection of a network's functional specialization in its age-specific structural covariance pattern. Based on previous findings, we hypothesized that the distributed neurocognitive default, dorsal attention, frontoparietal control, and ventral attention networks would show an inverted U-shaped trajectory of increasingly distributed structural covariance in early development, before shifting to more local covariance in advanced aging. Following results reported by Li and colleagues (2013) of age-independent patterns of structural covariance in somatomotor and visual networks across the adult life span, we predicted no age-dependent patterns of structural covariance in these networks. To examine these hypothesized life span trajectories, whole-brain structural covariance was assessed in a seed-based multivariate analysis (Persson et al., 2014; Spreng & Turner, 2013). This seed-based multivariate investigation allowed for the data-driven identification of significant age-related trajectories, based on the structural covariance of cortical gray matter with the chosen seed regions. We examine trajectories of structural covariance networks across the life span to consider what these changes might reveal about their developmental organization.

MATERIALS AND METHODS

In this study, our primary aim was to provide comprehensive mapping of the neurocognitive large-scale structural covariance networks across the entire life span. We collapsed cross-sectional data across five publicly available datasets to provide a normative sample ranging from 6 to 94 years of age. This also afforded us sufficient power for reliable estimates of structural covariance networks at six developmental epochs: Age Group 1 (6–15 years), Age Group 2 (16–25 years), Age Group 3 (26–35 years), Age Group 4 (36–59 years), Age Group 5 (60–75 years), and Age Group 6 (76–94 years). We assessed the structural covariance of six large-scale neurocognitive networks well represented in the literature: the default network (DN), dorsal attention network (DAN), frontoparietal control network (FPCN), somatomotor network (SM), ventral attention network (VAN), and visual systems.

Image Acquisition

Data were collated from five open-access data sources: National Institutes of Health Pediatric MRI Data Repository (NIH-Peds; Brain Development Cooperative Group & Evans, 2007): Release 5; Human Connectome Project (HCP): 500 subjects release; Nathan Kline Institute-Rockland Sample (NKI-RS; Nooner et al., 2012): Release 5; Open Access Series of Imaging Studies (OASIS); and Alzheimer's Disease Neuroimaging Initiative (ADNI). A complete listing of T1-weighted anatomical image acquisition procedures for each data source is provided in Table 1.

	Scanner			Flip				
	Strength (T)	TR (ms)	TE (ms)	TI (ms)	TD (ms)	Angle (deg.)	FOV (mm)	Voxel Size (mm)
NIH-Peds	1.5	22-25	10–11				$256 \times 160 - 180$	$1.0 \times 1.0 \times 1.0 - 1.5$
HCP	3	2,400	2.14	1,000	0	8	224×224	0.7 imes 0.7 imes 0.7
NKI-RS	3	1,900	2.52	900	0	9	250 imes 250	$1.0 \times 1.0 \times 1.0$
OASIS	1.5	9.7	4.0	20	200	10	256 imes 256	$1.0 \times 1.0 \times 1.25$
ADNI	1.5	2,400	min. full	1,000	0	8	240×240	0.94 imes 0.94 imes 1.2

 Table 1.
 Image acquisition parameters by data source

Participant Characteristics

From each sample, only healthy control participants older than six years of age with no diagnosed history of DSM (Diagnostic and Statistical Manual of Mental Disorders) Axis I or II disorder were considered. Six years was chosen as the lowest estimate for life span characterization, since previous work has indicated that normalization for children less than six years old is likely to introduce significant artifacts (Muzik, Chugani, Juhász, Shen, & Chugani, 2000), as gray matter volume in younger children is less than 95% of that observed in adults (Caviness, Kennedy, Richelme, Rademacher, & Filipek, 1996). For individuals meeting these criteria, the T1-weighted anatomical image was selected. In the case of longitudinal data, only the first time point was selected for each participant.

All T1-weighted anatomical images (n = 1,667) were visually inspected for quality assurance: images that showed evidence of artifacts were excluded (n = 87), yielding a final sample size of n = 1,580 (age M = 35 years, SD = 23 years, Range = 6–94 years; 659 males; 859 scanned at 1.5T and 721 at 3T). Participants were then sorted into the following age groups: Age Group 1 (6–15 years), Age Group 2 (16–25 years), Age Group 3 (26–35 years), Age Group 4 (36–59 years), Age Group 5 (60–75 years), and Age Group 6 (76–94 years). See Table 2 for sample sizes and participant characteristics by age group.

Segmentation and Preprocessing

Each age group was separately submitted to voxel-based morphometry (Ashburner & Friston, 2000) using the VBM8 toolbox (Kurth, Luders, & Gaser, 2010) implemented in Matlab (MATLAB 8.0, MathWorks, Natick, MA, 2012). Images were first segmented into gray matter, white matter, and cerebrospinal fluid using an extension of the New Segmentation algorithm. Gray matter images for this age group were then affine registered to the MNI template and carried to the Diffeomorphic Anatomical Registration through Exponentiated Lie Algebra toolbox (DARTEL; Ashburner, 2007), where they were iteratively aligned to create an age-group-specific template in MNI space. The six resulting age-group-specific templates were themselves then iteratively aligned again using DARTEL to create a study-specific template in MNI space. Importantly, this study-specific template equally weighted each of the age ranges represented by the six age groups.

Finally, previously segmented images were aligned to the study-specific template of interest using DARTEL high-dimensional normalization within VBM8. Nonlinear-only modulation was applied to gray matter images to derive regional differences in gray matter volume, correcting for total intracranial volume. Modulated gray matter images were iteratively smoothed to 8 mm FWHM (full width at half maximum) using *3dBlurToFWHM* in AFNI (Cox, 1996) and carried forward for further analysis.

able 2. Fullepart characteristics by age group							
	Sample Size	Age in Years	Scanned at				
Age Group	(Males)	M (SD)	1.5T/3T				
6–15 years	330 (159)	10 (2.66)	306/24				
16–25 years	302 (139)	21 (2.8)	176/126				
26–35 years	472 (192)	30 (2.74)	31/441				
36–59 years	139 (38)	49 (6.29)	68/71				
60–75 years	203 (82)	70 (4.16)	157/46				
76–94 years	134 (49)	81 (4.28)	121/13				

Table 2. Participant characteristics by age group

Network Identification

In this study, we sought to examine the structural covariance of the large-scale neurocognitive networks, including the DN, DAN, FPCN, SM, VAN, and visual networks. To examine each of these six networks, gray matter volumes for selected high-confidence seeds reported in Yeo et al. (2011) were extracted. Although Yeo and colleagues (2011) report high-confidence seeds for seven networks, we chose to exclude the reported "limbic network" as recent work has raised concerns regarding its test-retest reliability (Holmes et al., 2015).

For each of the six remaining networks we selected the top two high-confidence seeds reported by Yeo et al. (2011) as well as the contralateral seed regions, where contralateral seeds were chosen by changing the sign of the x-coordinate on each of the original high-confidence seeds. An exception to this procedure was made for the DN, which is known to separate into anterior and posterior components (Uddin, Kelly, Biswal, Castellanos, & Milham, 2009). Therefore, for the DN we selected the highest confidence seed and its contralateral seed. We then selected the second-highest confidence seed in posterior cingulate cortex as well as the fourth-highest confidence seed in medial prefrontal cortex, in order to ensure that both the anterior and the posterior DN components were represented in structural covariance estimates. A listing of all 24 seeds for the six networks examined is presented in Table 3 along with their respective anatomical label, and a visual representation of their location on cortex is presented in Figure 1.

Network Affiliation	X	у	Z	Laterality	Anatomical Label
Default	-7	49	18	L	Medial prefrontal cortex
	-7	-52	26	L	Posterior cingulate cortex
	-41	-60	29	L	Inferior parietal lobule
	41	-60	29	R	Inferior parietal lobule
Dorsal attention	-22	-8	54	L	Frontal eye fields
	22	-8	54	R	Frontal eye fields
	-51	-64	-2	L	Middle temporal motion complex
	51	-64	-2	R	Middle temporal motion complex
Frontoparietal control	-40	50	7	L	Frontal pole
	40	50	7	R	Frontal pole
	-43	-50	46	L	Anterior inferior parietal lobule
	43	-50	46	R	Anterior inferior parietal lobule
Ventral attention	-5	15	32	L	Anterior cingulate cortex
	5	15	32	R	Anterior cingulate cortex
	-31	11	8	L	Anterior insula
	31	11	8	R	Anterior insula
Somatomotor	-41	-20	62	L	Precentral gyrus (hand)
	41	-20	62	R	Precentral gyrus (hand)
	-55	-4	26	L	Precentral gyrus (tongue)
	55	-4	26	R	Precentral gyrus (tongue)
Visual	-3	-74	23	L	Extrastriate visual cortex
	3	-74	23	R	Extrastriate visual cortex
	-16	-74	7	L	Visual area 1
	16	-74	7	R	Visual area 1

Table 3.Selected seeds for each network

Coordinates (x, y, z) are in MNI stereotaxic space.

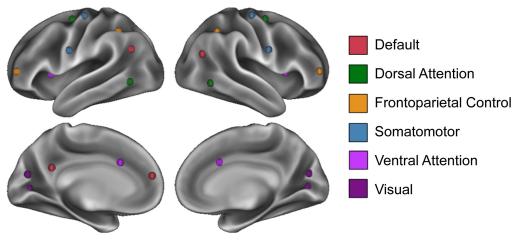


Figure 1. Selected seeded regions. The four selected seeded regions for each of the six neurocognitive networks are depicted in colors corresponding to their Yeo et al. (2011) labeling.

For each seed, gray matter volumes were extracted from a 10.5 mm edge cubical region of interest (ROI). Extracted gray matter volumes were then averaged across the four seeds for each participant. We chose to average gray matter volumes from multiple seeds to provide reliable, long-range estimates of network-specific structural covariance. This is in contrast to the more local estimates of structural covariance provided by gray matter volume from a single seed region. All six neurocognitive networks were examined by averaging the extracted gray matter volumes for each of the network-specific seeds, resulting in a $1,580 \times 1$ vector for each network. For each of the analyses, this vector **Y** represented the average gray matter volume for each participant of key nodes within the network. The resulting **Y** vectors were submitted to partial least squares (PLS; McIntosh, Bookstein, Haxby, & Grady, 1996). Additionally submitted to PLS were matrices of participant structural images, **X**, where **X** is an *N* subjects $\times N$ voxels matrix representing voxel-wise estimates of gray matter volume for each participant.

Partial Least Squares Analyses

PLS is a data-driven multivariate statistical technique capable of identifying patterns of structural covariance (Persson et al., 2014; Spreng & Turner, 2013). We utilized seed PLS to identify patterns of covariance between gray matter integrity in seed regions and whole-brain structural MRI images (for a review, see Krishnan, Williams, McIntosh, & Abdi, 2011). Here, we adopt the nomenclature used in Mišić et al. (2016).

Derivation of covariance matrix. For experimental analyses, our seed value was the average gray matter volume of four selected high-confidence seeds reported in Yeo et al. (2011). The vector **Y** representing this average gray matter volume was cross-correlated with a matrix **X** of participant's structural images. Importantly, this participant image matrix contained six submatrices $X_{1..6}$ corresponding to each age group. We retained this age group organization in our PLS analyses in order to directly compare age groups in their structural covariance between average network and whole-brain gray matter volume. The vector **Y** can therefore be considered as containing six subvectors, corresponding to the participant age groups. Both the gray matter volume vector and the image matrix were centered and normalized within age groups such that their cross-correlation resulted in a covariance vector **Z** according to the following:

$$Y_{1..6}{}^T X_{1..6} = Z_{1..6}. \tag{1}$$

Partial least squares: Multivariate decomposition technique used to identify shared patterns of covariance. Note that this covariance vector is equivalent to a correlation vector because of the described within-group normalization. The resulting covariance vector **Z** measures the degree to which the network average and whole-brain gray matter volumes covary at a voxel-wise level across participants.

Singular value decomposition. Using singular value decomposition (SVD; Eckart & Young, 1936), the covariance vector **Z** from Equation 1 was then decomposed into the following:

$$\mathbf{Z}_{1..6} = \boldsymbol{U} \boldsymbol{\Delta} \boldsymbol{V}^T, \tag{2}$$

where **V** is the orthonormal matrix of right singular vectors, **U** is the orthonormal matrix of left singular vectors, and Δ is the diagonal matrix of singular values. The right and left singular vectors represent the gray matter seed integrity profiles and spatial patterns that best characterize the covariance vector **Z**. The triplet of the right and left singular vectors and the singular values forms a set of mutually orthogonal latent variables (LVs), where the number of LVs derived is equal to the rank of the covariance vector **Z**. In our analyses, this identified six LVs for each network corresponding to the six submatrices of **Z**. Each LV was tested for statistical significance with 5,000 permutations and cross-validated for reliability with 1,000 bootstraps. Bootstrap ratios, derived from dividing the weight of the singular-vector by the bootstrapped standard error, are equivalent to *z* scores and were used to threshold significant LV spatial patterns at a 95% confidence interval for projection and interpretation.

Patterns were considered for further analysis based on two criteria. First, LVs must be statistically significant by permutation testing at the level of p < 0.001. Second, LVs must account for a minimum of 5% of the covariance in the data.

Derivation of subject scores. We also quantified individual contributions to each LV by deriving subject scores. Of particular interest in this work are the subject scores known in PLS nomenclature as "brain scores," which assess the contribution of each individual to the group structural covariance pattern. Multiplying the original matrix $X_{1..6}$ of participant structural images by the matrix of right singular vectors V derives these brain scores as follows:

$$L = X_{1..6}V, \tag{3}$$

where **L** is a matrix of brain scores. Recall from Equation 2 that the right singular vector **V** represents the seed-integrity profiles that best characterize the covariance matrix **Z**, such that multiplying this singular vector by the participant structural images derives the seed integrity profiles for each participant that reflect their contribution to the group structural covariance pattern. The matrix of brain scores **L** was extracted for each LV where, for each participant, this brain score value represents a weighted value of gray matter integrity within the regions identified in the group image.

By correlating brain score values for all subjects within each of the six age groups with their input gray matter integrity values, we were able to assess gray matter integrity in these regions for each age group separately. Computed confidence intervals on these correlations provide a means to assess the reliability of the structural covariance patterns in each age group; confidence intervals that cross zero are considered unreliable and are not interpreted in the results. To account for potential confounds, we ran a multiple regression of these brain scores controlling for scanner strength and gender. Although we present results (see Supplementary Figure 1 for an exemplar network; DuPre & Spreng, 2017). Corrected brain scores were plotted

Latent variables:

Linear combinations of the input variables that optimally explain orthogonal patterns of covariance.

Brain scores:

In partial least squares nomenclature, values measuring the extent to which an individual aligns with or contributes to the group spatial pattern. The value is taken as the dot product of the group result and the individual subject gray matter images. against age to visualize the covariance of the associated spatial pattern across the population. Because of the heterogeneity of resulting age-dependent trajectories, summary statistics for models fit to these corrected brain scores are available in Supplementary Tables 1 and 2 (DuPre & Spreng, 2017). For those models who show a "peak" in their age-dependent trajectory, the age at which this functional maximum occurs is noted in Supplementary Table 2.

RESULTS

We investigated the structural covariance of previously identified large-scale neurocognitive networks including the DN, DAN, FPCN, SM, VAN, and visual networks. Using PLS, we identified patterns of structural covariance for each of the six networks examined.

Neurocognitive Network Structural Covariance Patterns

PLS analyses of each of the large-scale networks examined yielded multiple significant latent variables (LVs), corresponding to reliable patterns of structural covariance within each network. We review significant results for each of the networks in turn.

Default network. Two significant LVs were identified for the DN and are presented in Figure 2. In the first LV (p < 0.0002; 61.57% covariance explained), seeded regions, along with homologous contralateral regions, covary together as well as with parahippocampal cortex and lateral temporal cortex (Figure 2A). Covariance extended to noncanonical DN regions including posterior insula. All age groups showed a robust positive association with this pattern (Figure 2B); this suggests that this latent variable corresponds to the structural covariance of the DN as it is preserved across the life span. Extracted brain scores (Figure 2C) revealed that the integrity of this structural covariance pattern declines with advancing age rapidly before reaching a plateau at approximately 70 years of age.

The second significant LV (p < 0.0002; 13.71% covariance explained) showed structural covariance patterns of developmental change in the DN. Age Group 2 (16–25 years) showed a unique pattern of increased structural covariance with medial prefrontal cortex and anterior insula compared with all other age groups examined (Figure 2D, 2E). Age groups with reliable correlations of brain scores and behavior—those for which the confidence interval did not cross zero and were therefore considered interpretable—included the Age Group 1 (6–15 years), Age Group 3 (26–35 years), Age Group 5 (60–75 years), and Age Group 6 (76–94 years) cohorts. Compared with Age Group 2 (16–25 years), each of these cohorts showed relatively increased structural covariance between seeded DN regions and sensorimotor structures, including motor and visual cortices as well as thalamus. Across the life span, this pattern shows a nearly linear decrease with advancing age (Figure 2F), suggesting that older adults are less strongly aligning to the structural covariance pattern depicted in Figure 2D.

Dorsal attention network. Two significant LVs were identified for the DAN and are presented in Figure 3. In line with results presented for the DN, the first significant DAN LV (p < 0.0002; 70.93% covariance explained) showed seeded regions positively covarying together as well as with canonical DAN regions such as intraparietal sulcus (Figure 3A). Covariance also extended to other, noncanonical DAN regions, including posterior insula and subgenual cingulate. All age groups showed a robust association with this pattern (Figure 3B). Brain scores reveal that the integrity of this pattern shows rapid decline with advancing age before plateauing at approximately 70 years (Figure 3C).

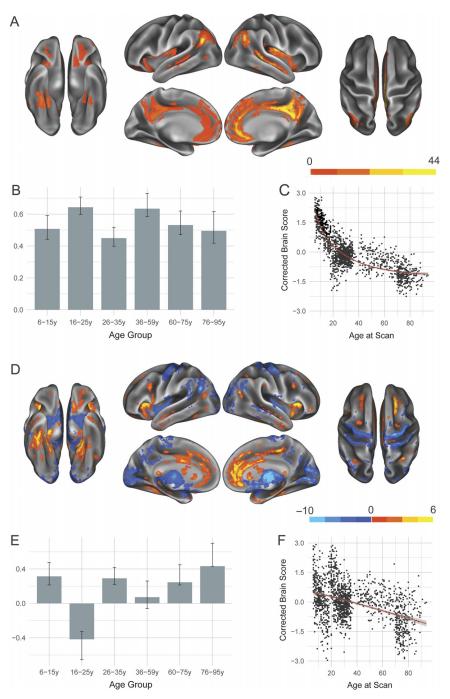


Figure 2. Structural covariance of the default network. (A) The spatial pattern for the first latent variable, thresholded at 95% of the bootstrap ratio. (B) The bootstrapped correlation of brain scores with the averaged gray matter volume estimates of default network seeds by age group for the first latent variable. (C) The individual brain scores from the first latent variable corrected for scanner strength and gender are plotted as a function of age. (D) Spatial pattern for the second latent variable, thresholded at 95% of the bootstrap ratio. (E) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of default network seeds by age group for the second latent variable, thresholded at 95% of the bootstrap ratio. (E) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of default network seeds by age group for the second latent variable. (F) The individual brain scores from the second latent variable corrected for scanner strength and gender are plotted as a function of age.

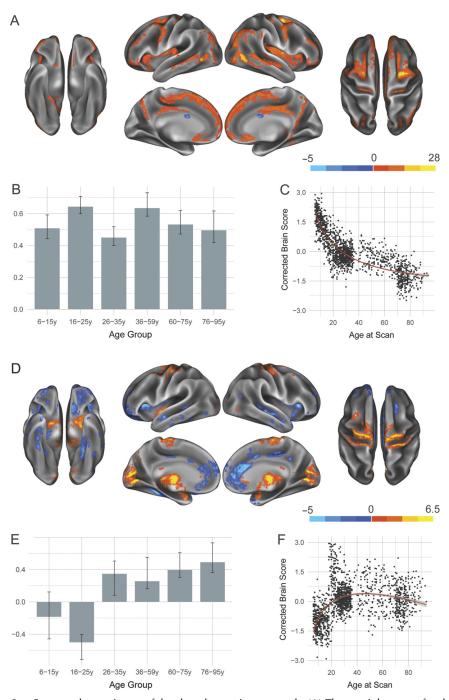


Figure 3. Structural covariance of the dorsal attention network. (A) The spatial pattern for the first latent variable, thresholded at 95% of the bootstrap ratio. (B) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of dorsal attention network seeds by age group for the first latent variable. (C) The individual brain scores from the first latent variable corrected for scanner strength and gender are plotted as a function of age. (D) Spatial pattern for the second latent variable, thresholded at 95% of the bootstrap ratio. (E) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of dorsal attention network seeds for the second latent variable, thresholded at 95% of the bootstrap ratio. (E) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of dorsal attention network seeds for the second latent variable. (F) The individual brain scores from the second latent variable corrected for scanner strength and gender are plotted as a function of age.

The second significant LV (p < 0.0002; 9.52% covariance explained) revealed developmental changes in the structural covariance pattern of the DAN. Age Group 2 (16–25 years) showed uniquely increased structural covariance with medial prefrontal cortex and anterior insula. Older age groups show relatively increased structural covariance between the seeded DAN regions and areas including motor and visual cortices as well as subcortical structures. Inspection of brain scores (Figure 3F) reveals an inverted U-shaped trajectory, with integrity of the structural covariance pattern reaching its peak in middle adulthood, while very young and very old individuals show significantly less integrity for the derived group structural covariance patterns.

Frontoparietal control network. Two significant LVs were identified for the FPCN and are depicted in Figure 4. Similar to results seen for the DN and DAN, the first significant LV (p < 0.0002; 78.05% covariance explained) showed a structural covariance pattern that was positively associated with all examined age groups, but showed a nonlinear decline in integrity across the life span. Seeded FPCN regions positively covary together, as well as with structures consistently associated with cognitive control, such as lateral prefrontal cortex, and noncanonical FPCN regions, such as posterior insula.

The second LV (p < 0.0002; 7.96% covariance explained) revealed developmental trajectories of structural covariance patterns in the FPCN. There was a significant dissociation between Age Groups 1 and 2 (6–25 years) as compared with middle and late Age Groups 4 and 5 (36–75 years). Younger age groups show increased structural covariance with structures both within the canonical FPCN such as precuneus as well as with noncanonical regions such as lateral temporal cortex. Older age groups, however, show relatively increased structural covariance for sensorimotor structures such as motor cortex and thalamus. Brain scores suggest an inverted U-shaped trajectory similar to that seen for the DAN, with the integrity of the structural covariance pattern at its highest levels in middle adulthood.

Somatomotor network. Two significant LVs were identified for the SM and are depicted in Figure 5. In agreement with the previously reported networks, the first significant LV (p < 0.0002; 72.91% covariance explained) showed a structural covariance pattern that is positively associated with all examined age groups and shows a nonlinear decline with advancing age. Seeded regions covaried together as well as with the motor strip. Covariance extended to areas outside the canonical motor network such as lateral prefrontal cortex and subcortical regions.

The second LV (p < 0.0002; 9.17% covariance explained) showed a significant dissociation between Age Groups 1 and 2 (6–25 years) as compared with Age Groups 4, 5, and 6 (36– 94 years). Younger age groups show increased structural covariance with structures outside of the canonical motor network such as lateral temporal cortex and mid-insula, while older age groups show relatively increased structural covariance local to the seed regions and to thalamus. Similar to the individual subject score trajectories seen for the DAN and FPCN, there is an inverted U-shaped trajectory in the integrity of this structural covariance pattern, with integrity reaching a peak in middle adulthood before beginning to decline.

Ventral attention network. Two significant LVs were identified for the VAN and are presented in Figure 6. The first LV (p < 0.0002; 70.93% covariance explained) again shows a structural covariance pattern positively associated with all examined age groups. Seeded VAN regions positively covary together and with the mid- and posterior insula as well as with the medial

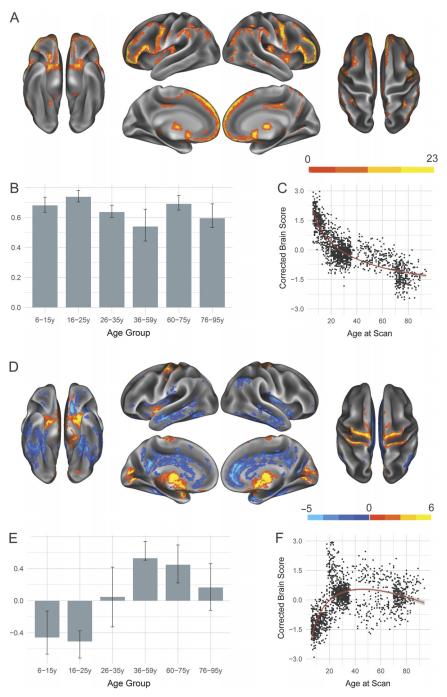


Figure 4. Structural covariance of the frontoparietal control network. (A) The spatial pattern for the first latent variable, thresholded at 95% of the bootstrap ratio. (B) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of frontoparietal control network seeds. (C) The individual brain scores from the first latent variable corrected for scanner strength and gender are plotted as a function of age. (D) Spatial pattern for the second latent variable, thresholded at 95% of the bootstrap ratio. (E) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of brain scores with averaged gray matter volume estimates of default network seeds by age group for the second latent variable. (F) The individual brain scores from the second latent variable corrected for scanner strength and gender are plotted as a function of age.

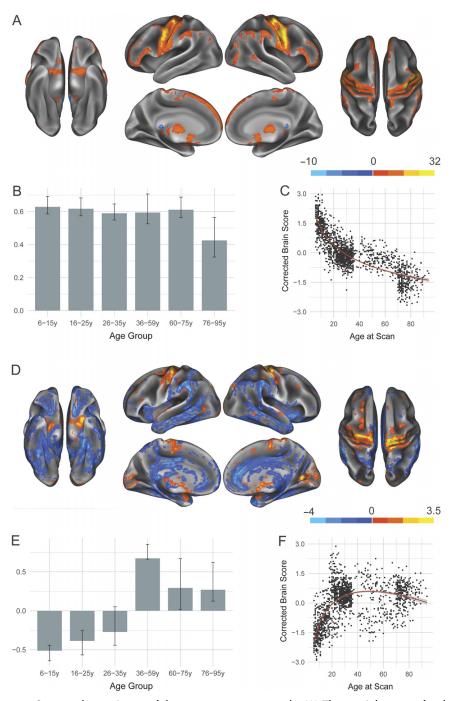


Figure 5. Structural covariance of the somatomotor network. (A) The spatial pattern for the first latent variable, thresholded at 95% of the bootstrap ratio. (B) The bootstrapped correlation of brain scores with bootstrapped averaged gray matter volume estimates of somatomotor network seeds by age group for the first latent variable. (C) The individual brain scores from the first latent variable corrected for scanner strength and gender are plotted as a function of age. (D) Spatial pattern for the second latent variable, thresholded at 95% of the bootstrap ratio. (E) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of somatomotor network seeds by age group for the second latent variable. (F) The individual brain scores from the second latent variable corrected for scanner strength and gender are plotted as a function of age.

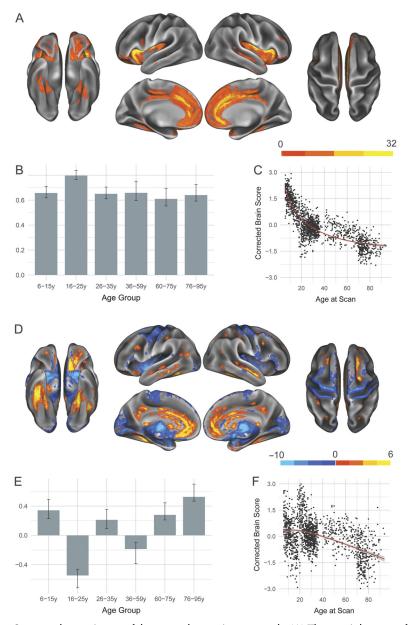


Figure 6. Structural covariance of the ventral attention network. (A) The spatial pattern for the first latent variable, thresholded at 95% of the bootstrap ratio. (B) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of ventral attention network seeds by age group for the first latent variable. (C) The individual brain scores from the first latent variable corrected for scanner strength and gender are plotted as a function of age. (D) Spatial pattern for the second latent variable, thresholded at 95% of the bootstrap ratio. (E) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of ventral attention network seeds by age group for the second latent variable. (F) The individual brain scores from the second latent variable corrected for scanner strength and gender are plotted as a function of age.

prefrontal cortex. Extracted brain scores revealed a nonlinear decline in the integrity of this structural covariance pattern across the life span.

The second significant LV (p < 0.0002; 13.83% covariance explained) revealed a pattern of developmental change similar to that seen in DN, with individuals in Age Group 2

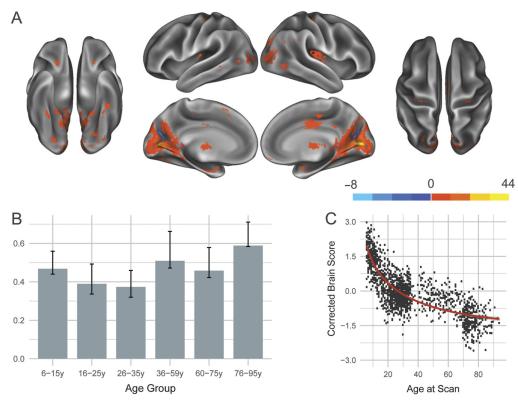


Figure 7. Structural covariance of the visual network. (A) The spatial pattern for the first latent variable, thresholded at 95% of the bootstrap ratio. (B) The bootstrapped correlation of brain scores with averaged gray matter volume estimates of visual network seeds by age group for the first latent variable. (C) The individual brain scores from the first latent variable corrected for scanner strength and gender are plotted as a function of age.

(16–25 years) and Age Group 4 (36–59 years) showing a unique structural covariance pattern compared with all other age groups. Specifically, these two groups showed increased structural covariance with medial prefrontal as well as parahippocampal cortex. Other age groups showed increased structural covariance with sensorimotor structures such as motor and visual cortices. Similarly to the DN, there is a near linear decrease in structural integrity across the life span, with older adults showing decreased structural covariance between seeded VAN regions and sensorimotor structures.

Visual network. One significant LV (p < 0.0002; 58.28% covariance explained) was identified for the visual network and is presented in Figure 7. As in previous networks, the significant LV revealed a structural covariance pattern that was positively associated with all examined age groups and nonlinearly declined with age. Seeded visual regions showed positive structural covariance with visual cortex as well as with noncanonical visual regions such as the posterior insula and mid-cingulate.

DISCUSSION

In this study, we examined the life span trajectories of structural covariance with publicly available cross-sectional data. For the six neurocognitive networks examined, our results revealed two broad developmental patterns: a stable pattern of structural covariance that

reflects network-specific features and persists across the life span, and an age-dependent pattern of structural covariance that reveals shared age-related trajectories of structural covariance across networks.

Persistent Patterns of Structural Covariance

Across all networks, the first significant latent variable identified a structural covariance pattern whose spatial extent was unique to the network of interest and persisted across age groups. Despite the stability of these structural covariance patterns over the life span, inspection of individual subject or "brain" scores (panel C, Figures 2–7) revealed that integrity of these patterns declines rapidly with advancing age before plateauing at approximately 70 years.

These findings extend on previous work showing a sharp decline in within-network structural covariance from young adulthood to middle age that persists into older adulthood (Li et al., 2013). Although our results show that network-specific structural covariance patterns were stable across the life span, we find that children and adolescents show even higher levels of integrity to these structural covariance patterns compared with young adults. This decline in integrity to structural covariance patterns over the life span may be related both to the increase in myelination across early development and its effects on gray-white matter tissue contrast (Lenroot & Giedd, 2006), as well as to the decline of cortical gray matter volume with age (Allen, Bruss, Brown, & Damasio, 2005).

Age-Dependent Patterns of Structural Covariance

In addition to stable patterns of structural covariance, DN, DAN, FPCN, SM, and VAN networks showed an additional, age-dependent pattern that differentiated young adulthood from either end of the life span.

Examination of brain scores in the DAN, FPCN, and SM (panel F, Figures 3–5) reveals that these align with an inverted U-shaped trajectory. These latent variables also showed overlapping features of structural covariance at a group level (panel D of Figures 3–5). In young adulthood, seeded regions showed structural covariance with areas including medial prefrontal cortex, posterior cingulate, insular cortex, and temporal cortex—association cortices corresponding to functional hubs (van den Heuvel & Sporns, 2013). In both childhood and older adulthood, however, seeded regions showed structural covariance with sensorimotor structures including motor and visual cortices and thalamus. These findings support previous work showing that structural covariance networks grow increasingly distributed over early development before shifting to a more localized topology in advanced aging (Wu et al., 2012). Our results in the DAN, FPCN, and SM suggest that distributed patterns of structural covariance networks are returning to a relatively localized topology in older adulthood.

The second significant latent variables of the DN and VAN share spatial features of structural covariance with the second latent variables of the DAN, FPCN, and SM; however, their trajectories (panel F, Figures 3 and 6) do not show a reliable, inverted U-shape. One possible explanation for this is that the selected seed regions for the DN and VAN included regions such as the medial prefrontal cortex, posterior cingulate, and insular cortex. These regions are known functional hubs (van den Heuvel & Sporns, 2013) and, in the second latent variable of DAN, FPCN, and SM, their structural covariance reliably differentiates young adulthood from other portions of the life span. In PLS, successive latent variables contribute unique, additional portions of variance. Since these seed regions strongly contribute to the structural covariance of the DN and VAN first latent variables, it is possible that the appearance of a near linear decline in the second latent variable—rather than an inverted U-shaped trajectory—is due to the exclusion of medial prefrontal cortex, posterior cingulate, and insular cortex from the second latent variables of the DN and VAN and their explained covariance. This would suggest that these regions are particularly important in shaping age-dependent patterns of structural covariance.

Previous investigations of structural covariance have found variation in the extent to which networks show age-related changes. For example, relatively flat patterns of structural covariance across adulthood have been seen in the visual network (Li et al., 2013) as well as in temporal, auditory, and cerebellar networks (Hafkemeijer et al., 2014). Our finding that the visual network did not have a significant second latent variable suggests that there is not a significant age-dependent pattern of structural covariance for this network, in agreement with this previous work.

Contrary to our initial hypotheses, we did find age-dependent structural covariance trajectories for SM, where existing literature suggests that there are little to no age-related changes (Li et al., 2013). In the present work, we find SM to exhibit the same age-dependent pattern of structural covariance as DAN and FPCN. Future longitudinal studies of structural covariance patterns will be important to address the impact of age on specific cortical networks.

Overall, our results therefore suggest that the structural covariance patterns of large-scale neurocognitive networks each have a unique spatial topology; however, neurocognitive networks also show overlapping patterns of age-dependent structural covariance.

Relationship of Structural Covariance to Function

Structural covariance networks have been extensively linked to neural function via their marked disruptions in pathology and pathological aging (Bassett et al., 2008; Hafkemeijer et al., 2016; Spreng & Turner, 2013; Valk, Martino, Milham, & Bernhardt, 2015). Alongside functional connectivity, shared structural covariance has been suggested as a defining characteristic of large-scale networks (Seeley, Crawford, Zhou, Miller, & Grecius, 2009; see also Di et al., 2017). It is worth considering, therefore, these life span patterns of structural covariance in light of the existing literature on the development of functional connectivity across the life span.

In our work, the first significant latent variable seen in all examined networks showed a stable pattern of structural covariance whose integrity declined across the life span. This is similar to patterns of decreasing within-network functional connectivity with advancing age (Betzel et al., 2014). The second latent variable seen in all networks—with the exception of the visual network—showed an age-dependent pattern that distinguished young adulthood from both childhood and advanced aging. These results mirror developmental trajectories commonly reported in functional connectivity studies with increased functional integration across networks in childhood, peak functional segregation between networks in young adulthood, and de-differentiation of network functional connectivity in older adulthood (Collin & van den Heuvel, 2013).

The significant overlap of structural covariance trajectories found in the current investigation and those trajectories reported in the functional connectivity literature suggest that a life span perspective may help illuminate the noted relationship between structural covariance and neural function. Directly assessing the relationship between structural covariance and functional connectivity, however, is a topic for future research aided by the collection of multimodal imaging data in life span samples (e.g., Glasser et al., 2016; Nooner et al., 2012).

Methodological Considerations

Although this study was able to leverage the increasing amount of anatomical data available in open-access repositories, it included important methodological considerations related to age group definition, scanner acquisition strength, and motion correction. Although we sought to create cohorts representing neurobiologically meaningful age ranges, this resulted in unequal representation in both sample size and age range considered. Our smallest included age group, Age Group 6 (76–94 years), included 134 participants, while our largest age group, Age Group 3 (26–35 years), included 472 participants. Although differing sample sizes across groups will invariably yield more variable estimates of group-wise covariance, we note that our estimates have statistical power comparable to the smallest group size considered. At 134 subjects, this is still significantly higher powered than current standards for MRI data collection, particularly in life span samples. An additional consideration with our selection of age cohorts is the age range considered in each age group. Age Group 4, defined here as ages 36-59, spans a larger time period than any of the other cohorts considered. This was in large part due to the paucity of openly available data for that cohort, particularly when compared with other cohorts such as younger adulthood. The continuing collection of multimodal data for life span initiatives such as NKI-RS (Nooner et al., 2012), the HCP Lifespan Project (Glasser et al., 2016), and UK Biobank (Miller et al., 2016) will increase the availability of high-quality data to investigate such questions.

Differences in scanner acquisition strength across data sources provide an additional important methodological consideration. Several data sources, including those representing the youngest and oldest subjects, were acquired at 1.5T, while young adults were acquired at 3T. Although it is likely that subtle differences between groups may have been introduced by MR field strength, inspection of individual subject scores from the two included life span data sources (OASIS and NKI-RS) indicate that these subjects do not show divergent results from those seen in the age-restricted datasets or from one another. This is suggestive of general agreement in structural covariance trends across scanner field strength, as OASIS was collected at 1.5T while NKI-RS was collected at 3T. Further, we controlled for MR field strength across groups by adjusting individually derived subject scores and found similar results for both raw and corrected subject scores. Future work assessing structural covariance across the life span should nonetheless aim to examine scans acquired at the same MR field strength and ideally on the same scanner.

A limitation of the current study is the inability to implement motion correction of structural images. Recent work has shown that head motion may introduce artifacts into anatomical images, affecting automated estimates of structure (Alexander-Bloch et al., 2016; Savalia et al., 2016). Although acquisition of a resting-state scan has been proposed to flag high-motion subjects for exclusion from structural analyses (Alexander-Bloch et al., 2016; Savalia et al., 2016), not all of the datasets utilized also provided at least one resting-state scan for each subject. We therefore caution that estimates of age group differences may be inflated by uncorrected motion. Each of these methodological considerations can be addressed in future work, as comprehensive samples of participants across the life span with both structural and functional imaging become increasingly available.

In this study we utilized open-access, cross-sectional data sources to examine structural covariance patterns of six neurocognitive networks across the life span. Using multivariate PLS analysis, we found that all networks exhibited stable patterns of network-specific structural covariance, and with the exception of the visual network showed a second, age-dependent pattern of structural covariance that mirrored developmental trends seen in the functional connectivity literature. The present results confirm the utility of structural covariance in defining neurocognitive networks and reveal both shared and network-specific trajectories of structural covariance across the life span.

ACKNOWLEDGMENTS

NIH Peds data used in the preparation of this article were obtained from the NIH Pediatric MRI Data Repository created by the NIH MRI Study of Normal Brain Development. This is a multisite, longitudinal study of typically developing children from ages newborn through young adulthood conducted by the Brain Development Cooperative Group and supported by the National Institute of Child Health and Human Development, the National Institute on Drug Abuse, the National Institute of Mental Health, and the National Institute of Neurological Disorders and Stroke (Contract numbers N01-HD02-3343, N01-MH9-0002, and N01-NS-9-2314, -2315, -2316, -2317, -2319, and -2320). A listing of the participating sites and a complete listing of the study investigators can be found at http://pediatricmri.nih.gov/ nihpd/info/participating_centers.html. HCP data were provided by the Human Connectome Project, WU-Minn Consortium (principal investigators: David Van Essen and Kamil Ugurbil; 1U54MH091657) funded by the 16 NIH Institutes and Centers that support the NIH Blueprint for Neuroscience Research; and by the McDonnell Center for Systems Neuroscience at Washington University. NKI data were obtained from the Nathan Kline Institute – Rockland Sample, Release 5. Principal support for the enhanced NKI-RS project was provided by the NIMH BRAINS R01MH094639-01 (principal investigator: Michael Milham). Funding for key personnel was also provided in part by the New York State Office of Mental Health and Research Foundation for Mental Hygiene. Funding for the decompression and augmentation of administrative and phenotypic protocols was provided by a grant from the Child Mind Institute (1FDN2012-1). Additional personnel support was provided by the Center for the Developing Brain at the Child Mind Institute, as well as NIMH R01MH081218, R01MH083246, and R21MH084126. Project support was also provided by the NKI Center for Advanced Brain Imaging (CABI), the Brain Research Foundation, and the Stavros Niarchos Foundation. OASIS data were supported by the following grants: P50 AG05681, P01 AG03991, R01 AG021910, P50 MH071616, U24 RR021382, R01 MH56584. ADNI data used in preparation of this article were obtained from the Alzheimer's Disease Neuroimaging Initiative (ADNI) database (http://adni.loni.usc.edu). As such, the investigators within the ADNI contributed to the design and implementation of ADNI and/or provided data but did not participate in analysis or writing of this report. A complete listing of ADNI investigators can be found at http://adni.loni.usc.edu/wp-content/uploads/how_to_apply/ADNI_Acknowledgement_List. pdf. Data collection and sharing for this project was funded by the Alzheimer's Disease Data collection and sharing for this project was funded by the Alzheimer's Disease Neuroimaging Initiative (ADNI) (National Institutes of Health Grant U01 AG024904) and DOD ADNI (Department of Defense award number W81XWH-12-2-0012). ADNI is funded by the National Institute on Aging, the National Institute of Biomedical Imaging and Bioengineering, and through generous contributions from the following: AbbVie; Alzheimer's Association; Alzheimer's Drug Discovery Foundation; Araclon Biotech; BioClinica, Inc.; Biogen; Bristol-Myers Squibb Company; CereSpir, Inc.; Eisai, Inc.; Elan Pharmaceuticals, Inc.; Eli Lilly and Company; EuroImmun; F. Hoffmann-La Roche, Ltd., and its affiliated company, Genentech, Inc.; Fujirebio; GE Healthcare; IXICO, Ltd.; Janssen Alzheimer Immunotherapy Research & Development, LLC.; Johnson & Johnson Pharmaceutical Research & Development, LLC.; Lumosity; Lundbeck; Merck & Co., Inc.; Meso Scale Diagnostics, LLC.; NeuroRx Research; Neurotrack Technologies; Novartis Pharmaceuticals Corporation; Pfizer, Inc.; Piramal Imaging; Servier; Takeda Pharmaceutical Company; and Transition Therapeutics. The Canadian Institutes of Health Research is providing funds to support ADNI clinical sites in Canada. Private sector contributions are facilitated by the Foundation for the National Institutes of Health (http://www.fnih.org). The grantee organization is the Northern California Institute for Research and Education, and the study is coordinated by the Alzheimer's Disease Cooperative Study at the University of California, San Diego. ADNI data are disseminated by the Laboratory of Neuro Imaging at the University of Southern California. This manuscript reflects the views of the authors and may not reflect the opinions or views of the NIH.

AUTHOR CONTRIBUTIONS

Elizabeth DuPre: Conceptualization; Formal analysis; Visualization; Writing – original draft. R. Nathan Spreng: Conceptualization; Formal analysis; Funding acquisition; Methodology; Supervision; Writing – original draft.

FUNDING INFORMATION

This work was supported in part by an Alzheimer's Association grant (NIRG-14-320049) to R.N.S.

REFERENCES

- Alexander-Bloch, A., Clasen, L., Stockman, M., Ronan, L., Lalonde, F., Giedd, J., & Raznahan, A. (2016). Subtle in-scanner motion biases automated measurement of brain anatomy from in vivo MRI. *Human Brain Mapping*, *37*, 2385–2397.
- Alexander-Bloch, A., Giedd, J. N., & Bullmore, E. (2013). Imaging structural co-variance between human brain regions. *Nature Reviews: Neuroscience*, 14, 322–336.
- Alexander-Bloch, A., Raznahan, A., Bullmore, E., & Giedd, J. (2013). The convergence of maturational change and structural covariance in human cortical networks. *Journal of Neuroscience*, 33, 2889–2899.
- Allen, J. S., Bruss, J., Brown, C. K., & Damasio, H. (2005). Normal neuroanatomical variation due to age: The major lobes and a parcellation of the temporal region. *NeuroImage*, *26*, 1245–1260.
- Ashburner, J. (2007). A fast diffeomorphic registration algorithm. *NeuroImage*, *38*, 95–113.
- Ashburner, J., & Friston, K. J. (2000). Voxel-based morphometry— The methods. *NeuroImage*, 11, 805–821.
- Bassett, D. S., Bullmore, E., Verchinski, B. A., Mattay, V. S., Weinberger, D. R., & Meyer-Lindenberg, A. (2008). Hierarchical organization of human cortical networks in health and schizophrenia. *Journal of Neuroscience*, 28, 9239–9248.
- Betzel, R. F., Byrge, L., He, Y., Goñi, J., Zuo, X. N., & Sporns, O. (2014). Changes in structural and functional connectivity among resting-state networks across the human lifespan. *NeuroImage*, *102*, 345–357.

- Brain Development Cooperative Group & Evans, A. C. (2007). The NIH MRI study of normal brain development. *NeuroImage*, *30*, 184–202.
- Caviness, J. V. S., Kennedy, D. N., Richelme, C., Rademacher, J., & Filipek, P. A. (1996). The human brain age 7–11 years: A volumetric analysis based on magnetic resonance images. *Cerebral Cortex*, 6, 726–736.
- Chan, M. Y., Park, D. C., Savalia, N. K., Petersen, S. E., & Wig, G. S. (2014). Decreased segregation of brain systems across the healthy adult lifespan. *Proceedings of the National Academy of Sciences*, 111, 4997–5006.
- Collin, G., & van den Heuvel, M. P. (2013). The ontogeny of the human connectome: Development and dynamic changes of brain connectivity across the life span. *Neuroscientist*, *19*, 616–628.
- Cox, R. W. (1996). AFNI: Software for analysis and visualization of functional magnetic resonance neuroimages. *Computers and Biomedical Research*, 29, 162–173.
- Di, X., Gohel, S., Thielcke, A., Wehrl, H. F., Biswal, B. B., & Alzheimer's Disease Neuroimaging Initiative. (2017). Do all roads lead to Rome? A comparison of brain networks derived from inter-subject volumetric and metabolic covariance and moment-to-moment hemodynamic correlations in old individuals. *Brain Structure and Function*. https://doi.org/10.1007/ s00429-017-1438-7
- Dosenbach, N. U. F., Nardos, B., Cohen, A. L., Fair, D. A., Power, J. D., Church, J. A., . . . Schlaggar, B. L. (2010). Prediction of individual brain maturity using fMRI. *Science*, 329, 1358–1361.

- DuPre, E., & Spreng, R. N. (2017). Supplemental material for "Structural covariance networks across the life span from 6 to 94 years of age." *Network Neuroscience*, *1*(3), 302–323. https://doi.org/10.1162/netn_a_00016
- Eckart, C., & Young, G. (1936). The approximation of one matrix by another of lower rank. *Psychometrika*, *1*, 211–218.
- Fjell, A. M., Westlye, L. T., Espeseth, T., Reinvang, I., Walhovd, K. B., Dale, A. M., & Holland, D. (2010). Cortical gray matter atrophy in healthy aging cannot be explained by undetected incipient cognitive disorders: A comment on Burgmans et al. (2009). *Neuropsychology*, 24, 258–266.
- Giorgio, A., Santelli, L., Tomassini, V., Bosnell, R., Smith, S., De Stefano, N., & Johansen-Berg, H. (2010). Age-related changes in grey and white matter structure throughout adulthood. *NeuroImage*, *51*, 943–951.
- Glasser, M. F., Smith, S. M., Marcus, D. S., Andersson, J. L. R., Auerbach, E. J., Behrens, T. E. J., . . . Van Essen, D. C. (2016). The Human Connectome Project's neuroimaging approach. *Nature Neuroscience*, *19*, 1175–1187.
- Hafkemeijer, A., Altmann-Schneider, I., de Craen, A. J. M., Slagboom, P. E., van der Grond, J., & Rombouts, S. A. R. B. (2014). Associations between age and gray matter volume in anatomical brain networks in middle-aged to older adults. *Aging Cell*, *13*, 1068–1074.
- Hafkemeijer, A., Möller, C., Dopper, E. G. P., Jiskoot, L. C., van den Berg-Huysmans, A. A., van Swieten, J. C., . . . Rombouts, S. A. R. B. (2016). Differences in structural covariance networks between behavioral variant frontotemporal dementia and Alzheimer's disease. *Human Brain Mapping*, *37*, 978–988.
- Hagmann, P., Sporns, O., Madan, N., Cammoun, L., Pienarr, R., Wedeen, V. J., . . . Grant, P. E. (2010). White matter maturation reshapes structural connectivity in the late developing human brain. *Proceedings of the National Academy of Sciences*, 107, 19067–19072.
- Holmes, A. J., Hollinshead, M. O., O'Keefe, T. M., Petrov, V. I., Fariello, G. R., Wald, L. L., . . . Buckner, R. L. (2015). Brain Genomics Superstruct Project initial release with structural, functional, and behavioral measures. *Scientific Data*, 2. https://doi. org/10.1038/sdata.2015.31
- Krishnan, A., Williams, L. J., McIntosh, A. R., & Abdi, H. (2011). Partial Least Squares (PLS) methods for neuroimaging: A tutorial and review. *NeuroImage*, 56, 455–475.
- Krongold, M., Cooper, C., & Bray, S. (2017). Modular development of cortical gray matter across childhood and adolescence. *Cerebral Cortex*, 27, 1125–1136.
- Kurth, F., Luders, E., & Gaser, C. (2010). VBM8 toolbox manual, http://www.neuro.uni-jena.de/vbm/
- Lenroot, R. K., & Giedd, J. N. (2006). Brain development in children and adolescents: Insights from anatomical magnetic resonance imaging. *Neuroscience & Biobehavioral Reviews*, 3(6), 718–729.
- Li, X., Pu, F., Fan, Y., Niu, H., Li, S., & Li, D. (2013). Age-related changes in brain structural covariance networks. *Frontiers in Human Neuroscience*, *7*. https://doi.org/10.3389/fnhum.2013. 00098
- Low, L. K., & Cheng, H.-J. (2006). Axon pruning: An essential step underlying the developmental plasticity of neuronal

connections. *Philosophical Transactions of the Royal Society B*, 361, 1531–1544.

- McIntosh, A., Bookstein, F., Haxby, J., & Grady, C. (1996). Spatial pattern analysis of functional brain images using partial least squares. *NeuroImage*, *3*, 143–157.
- Mechelli, A., Friston, K. J., Frackowiak, R. S., & Price, C. J. (2005). Structural covariance in the human cortex. *Journal of Neuroscience*, *25*, 8303–8310.
- Mesulam, M. M. (1998). From sensation to cognition. *Brain*, 121, 1013–1052.
- Miller, K. L., Alfaro-Almagro, F., Bangerter, N. K., Thomas, D. L., Yacoub, E., Xu, J., . . . Smith, S. M. (2016). Multimodal population brain imaging in the UK Biobank prospective epidemiological study. *Nature Neuroscience*, *19*, 1523–1536.
- Mišić, B., Betzel, R. F., de Reus, M. A., van den Heuvel, M. P., Berman, M. G., McIntosh, A. R., & Sporns, O. (2016). Networklevel structure-function relationships in human neocortex. *Cerebral Cortex*, *26*, 3285–3296.
- Montembeault, M., Joubert, S., Doyon, J., Carrier, J., Gagnon, J. F., Monchi, O., . . . Brambati, S. M. (2012). The impact of aging on gray matter structural covariance networks. *NeuroImage*, *63*, 754–759.
- Muzik, O., Chugani, D. C., Juhász, C., Shen, C. G., & Chugani, H. T. (2000). Statistical parametric mapping: Assessment of application in children. *NeuroImage*, *12*, 538–549.
- Nooner, K. B., Colcombe, S. J., Tobe, R. H., Mennes, M., Benedict, M. M., Moreno, A. L., . . . Milham, M. P. (2012). The NKI-Rockland sample: A model for accelerating the pace of discovery science in psychiatry. *Frontiers in Neuroscience*, 6. https://doi. org/10.3389/fnins.2012.00152
- Pagani, M., Bifone, A., & Gozzi, A. (2016). Structural covariance networks in the mouse brain. *NeuroImage*, *129*, 55–63.
- Persson, J., Spreng, R. N., Turner, G., Herlitz, A., Morell, A., Stening, E., . . . Söderlund, H. (2014). Sex differences in volume and structural covariance of the anterior and posterior hippocampus. *NeuroImage*, 99, 215–225.
- Raz, N., Lindenberger, U., Rodrigue, K. M., Kennedy, K. M., Head, D., Williamson, A., . . . Acker, J. D. (2005). Regional brain changes in aging healthy adults: General trends, individual differences and modifiers. *Cerebral Cortex*, 15, 1676–1689.
- Savalia, N. K., Agres, P. F., Chan, M. Y., Feczko, E. J., Kennedy, K. M., & Wig, G. S. (2016). Motion-related artifacts in structural brain images revealed with independent estimates of in-scanner head motion. *Human Brain Mapping*, 38, 472–492.
- Seeley, W. W., Crawford, R. K., Zhou, J., Miller, B. L., & Grecius, M. D. (2009). Neurodegenerative diseases target large-scale human brain networks. *Neuron*, 62, 42–52.
- Spreng, R. N., & Turner, G. R. (2013). Structural covariance of the default network in healthy and pathological aging. *Journal of Neuroscience*, *33*, 15226–15234.
- Tijms, B. M., Seris, P., Willshaw, D. J., & Lawrie, S. M. (2012). Similarity-based extraction of individual networks from gray matter MRI scans. *Cerebral Cortex*, 22, 1530–1541.
- Uddin, L. Q., Kelly, A. M. C., Biswal, B. B., Castellanos, F. X., & Milham, M. P. (2009). Functional connectivity of default mode

network components: Correlation, anticorrelation, and causality. *Human Brain Mapping*, *30*, 625–637.

- Valk, S. L., Martino, A. D., Milham, M. P., & Bernhardt, B. C. (2015). Multicenter mapping of structural network alterations in autism. *Human Brain Mapping*, *36*, 2364–2373.
- van den Heuvel, M. P., & Sporns, O. (2013). Network hubs in the human brain. *Trends in Cognitive Neurosciences*, *17*, 683–696.
- Wu, K., Taki, Y., Sato, K., Kinomura, S., Goto, R., Okada, K., . . . Fukuda, H. (2012). Age-related changes in topological organization of structural brain networks in healthy individuals. *Human Brain Mapping*, *33*, 552–568.
- Yeo, B. T. T., Krienen, F. M., Sepulcre, J., Sabuncu, M. R., Lashkari, D., Hollinshead, M., . . . Buckner, R. L. (2011). The organization of the human cerebral cortex estimated by intrinsic functional connectivity. *Journal of Neurophysiology*, *106*, 1125–1165.
- Zielinski, B. A., Gennatas, E. D., Zhou, J., & Seeley, W. W. (2010). Network-level structural covariance in the developing brain. *Proceedings of the National Academy of Sciences*, *107*, 18191– 18196.
- Zuo, X.-N., He, Y., Betzel, R. F., Colcombe, S., Sporns, O., & Milham, M. P. (2017). Human connectomics across the life span. *Trends in Cognitive Sciences*, *21*, 32–45.